



Numerical modeling in quantitative ultrasonic tomography of standing trees

Andrés Arciniegas, Loïc Brancheriau, Philippe Gallet, Philippe Lasaygues

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The aim of this project is to develop an ultrasonic device for parametric imaging of standing trees. The device is designed to perform both transmission and reflection measurements that can be therefore used for quantitative tomographic imaging. It allows various automatic acquisitions, since the angular position of the transducers could be adjusted. This makes possible to scan the wave propagation occurring in all directions inside the medium. The associated electronic set-up allows mainly measuring the slowness (and therefore the velocity) and the attenuation of the ultrasonic waves. Tomograms were computed by fast algebraic algorithms: (1) using the filtered backprojection algorithm with fan beam geometry, (2) using a new algorithm that we are developing based on a "layer-stripping" method. Our first numerical results on an academic and realistic phantom of tree are presented in this paper.

1 Introduction

The upward-growth structures on the standing trees are changing fast in order to compete for environmental strength and the natural weather forces, and obviously relatively to the age. These changes result in complex mechanical variations, and the physical properties result of gradual transition from juvenile to mature stage into the tree. In addition to naturally occurring material property variations, abnormal diseases content also varies from the pith to the bark. Anyway, healthy trees can present mechanical weaknesses, and therefore be dangerous in urban environments. Studies have demonstrated the effectiveness of acoustics in detecting/imaging trees' decay. The main commercial acoustic devices for tree assessment are essentially based on methods using low frequency acoustic waves. Three tools are "PICUS[®] Sonic Tomograph" (Germany) [1], the "ARBOTOM[®]" [2] (Germany), and the "FAKOPP" [3] (Hungary). They use an impulse hammer to excite the trunk and measure the acceleration on circumferential points (accelerometer) with a limited number of sensors. These methods give average values recorded along the acoustic pathway, but they are not always suitable to access 2D resolution (about few centimeters for defect size).

During the last decade, ultrasonic tomography made considerable progress in medical and industrial domain. With the evolution of the electro-acoustical technology new devices for image acquisition have appeared. The main aim of our project is to develop a mechanical ultrasonic imaging device for standing trees (ARB'UST) using two transducers (from 50 to 90 kHz), that could be transportable and used in an *in situ* condition. With ARB'UST, data is collected sending energy through the tree as many different angles as used to compute an image of the changes of a physical quantity in a slice. The ultrasonic waves cross from the emitter to the receiver at appropriate locations around the tree. These locations are chosen so that as many rays pass through as much of the object as possible. The parameter measured is the time-of-flight (travel time) of the ultrasonic wave between the emitter and the receiver. The final ultrasonic tomogram represents the slowness (the velocity) distribution (related to the axial and lateral resolution of the transducers) in a thin cross-section of the tree (related to the elevational resolution of the transducers).

In ultrasonic tomography different approaches have already been proposed in literature [4, 5, 6]. There are two major classes of reconstruction techniques. One class is based on the projection-slice theorem such as the filtered backprojection method (FBP). This method is fast and the data must be acquired on spaced sets of straight ray paths (projections). The main actual challenge in tree imaging is the choice of the effective method to inverse the scattered data, and the first step in this work is to test two tomographic inversion methods. This paper focus in an approach by numerical simulation

of the reconstructions of cylindrical homogeneous isotropic medium with defects.

2 Materials and methods

In this paper a comprehensive study is conducted on the reconstruction capability of travel time tomography method for a ring transducer scanner using computed-simulated data for a numerical tree phantom. The scheme to simulate ultrasonic-wave propagation through the phantom depends of the experimental set-up and assumptions.

From the mechanical point of view, ARB'UST device was designed to perform sectorial scanning such as fan beam or transmission mode. The general architecture of the system is that of an ultrasound tomographic scanner. An aluminum ring holds two 50 kHz - transducers allowing the bi-static 2D-survey around the trunk [7].

The numerical simulation can be used to study the accuracy of different travel time tomography for different tree phantoms (shapes and physical properties mimics). Numerical tree phantoms are placed inside a ring where transducers are positioned at the boundaries at regular angular spacing locations, from 0° to 360°. A 120° circular sector is not scanned due to positions where the receiver cannot be experimentally placed (Figure 1). A typical angular step of 4° leads to 61 points per projection. For a complete scan, the total number of acquisitions is therefore 5490. For one projection, the emitter remains in its position while the receiver moves around the ring (Figure 1).

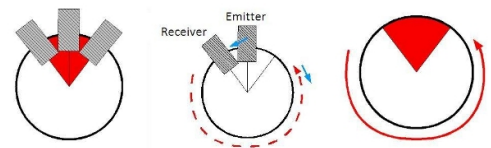


Figure 1: The principle of acquisition

For this purpose, pure compression ultrasonic wave were transmitted in the sample, and no shear waves were taken into account. The medium was supposed homogeneous and isotropic. The wave velocities were independent of frequency. The ultrasonic wave attenuation would be neglected. Only the propagation path phenomena were considered, and the wave delays studied. The numerical tree phantom was then represented by the ultrasonic slowness distribution, and each pixel had a constant value of slowness of the ultrasonic wave. The implementation of the phantom, algorithms and simulations was made in MATLAB[®].

2.1 Mimicking phantom of tree

Simulations can be easily performed for a large number of well-controlled mimicking phantoms of tree, and can help to understand the features of wavefields acquired by transducers. The simulation can then be used to study the accuracy of travel time tomography for different sizes and shapes of phantom. In this paper, it is proposed to apply this method for a phantom having two main perturbation sizes and shapes inside the host medium and including a small defect. The numerical phantom is a cylindrical homogeneous isotropic object, with cylindrical homogeneous isotropic perturbations (Figure 2). Each small point at the boundaries of the object represent an angular position where the emitter is going to be placed. Table 1 shows the parameters used to construct the phantom.

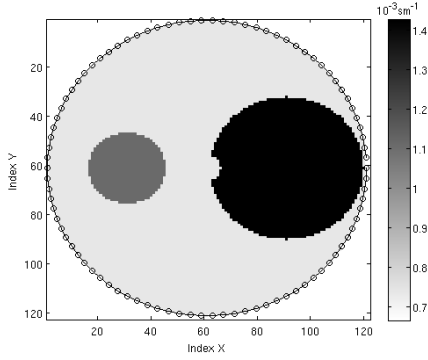


Figure 2: Numerical phantom. o : Positions where the sensors are going to be experimentally placed.

Table 1: Parameters of the phantom

Diameter (in pixels)	Position	Slowness (10^{-3} sm^{-1})	Velocity (ms^{-1})
122	centered	0.74	1350
28	off-centered	1.11	900
58	off-centered	1.43	700

2.2 Forward problem

To test the reconstruction algorithms, it was carried out a numerical implementation of the experimental protocol (acquisition sequences). Equation 1 is known as the Radon transform of a function $f(x, y)$.

$$P_{\theta}(\tau) = \int_{(\theta, \tau) \text{ line}} f(x, y) ds \quad (1)$$

In the reality, the function f represents the physical parameter to be measured. For a fan beam geometry, an independent measurement, or point of projection, is defined as the ray integral (along the line τ) as is given by $P_{\theta}(\tau)$ for a constant observation angle θ [4]. A projection is therefore the collection of the ray integrals measured along the fan.

Travel time t between an emitter n and a receiver m is represented by a line integral of the slowness p along the ray path Γ [8], as shown in Eq. 2.

$$t(n, m) = \int_{\Gamma(n, m)} p(x, y) d\Gamma \quad (2)$$

The discrete forward problem for an independent travel time measurement is then approximated by a weighted summation for N pixels crossed by a given ray path (Eq. 3).

$$t(n, m) = \sum_{q=1}^N p_q d_q \quad (3)$$

The distance D for a given path is assumed as a multiple of constant discrete step d_q (pixel), thus $D = Nd_q$. Dividing each side of Eq. 3 by D , the numerical implementation of Radon transform for the slowness $P(n, m)$ is then:

$$P(n, m) = \frac{1}{N} \sum_{\Gamma(n, m)} p(x, y) \quad (4)$$

2.3 Reconstruction by the filtered backprojection method (reference method)

Let us consider a mesh of pixels. To find the value of the slowness at any point of the object, it is assigned the value of the projection at any pixel placed in the path that it covers, and then adding all contributions from all projections. This principle is called backprojection. This method, however, leads to biased values and it is necessary to correct each projection by a specific filtering. The filtered backprojection consists therefore initially to filter each projection using a ramp filter (often combined with a low pass filter to avoid noise amplification), and then to project back the filtered projections for the different observation angles [4].

2.4 Reconstruction by the Layer Stripping based method

In this paper, it is proposed an application of a new inversion algorithm based on a "Layer Stripping" method [9]. This procedure is an iterative approach, for transmission measurements in fan-beam mode, where ray paths are analyzed as if the object was discretized by concentric layers. The tomographic reconstruction consists of the local estimation of slowness of an identified concentric layer and to correct it with respect to the values of slowness that were already calculated in the previous layers. Analysis towards the center leads the evolution of the reconstruction. This multi-layer approach is adapted to the tree because their circumferential cross section, from internal to external, can be associated to a 2D annular structure.

2.4.1 Discretization

The number of layers depends on the number of transducers. N (pair) transducers are distributed uniformly around the object every $360^\circ / N$ (angular step). Equation 5 shows that the value of the radius of a layer is determined by:

$$d(k) = \min_{M \in D} |C - M|; \forall 1 \leq k \leq N/2; k \in \mathbb{N} \quad (5)$$

Where:

$d(k)$: the distance from the layer k towards the center (radius of the layer). Thus the mesh is composed by $N/2$ layers.

C : is the center of the object.

D : the straight ray linking transducers $E_1 E_{k+1}$

M : point in D

2.4.2 Algorithm

Let Eq. 6 describe the slowness for a simple backprojection process. Γ is the straight ray connecting the emitter $E(n)$ to the receiver $E(m)$. $\Omega(i, j)$ the set of straight rays that intersect a pixel at (i, j) , where i and j are the index of the resulting image by the reconstruction¹. $|\Omega|$ is the number of straight rays of the set.

$$p(i, j) = \frac{1}{|\Omega|} \sum_{\Omega(i, j)} P(n, m) \quad (6)$$

From the forward problem, and assuming the existence of nested layers, Eq. 4 could be explained by Eq. 7.

$$NP(n, m) = \sum_{\text{layer } k-1} p_{k-1}(i, j) + \sum_{\text{layer } k} p_k(i, j) \quad (7)$$

A generalization of Eq. 4 leads to the slowness P of a layer. Slowness at a layer $k-1$ and k is then estimated as shown in Eq. 8 and Eq. 9.

$$\sum_{\text{layer } k-1} p_{k-1}(i, j) = N_{k-1} P_{k-1} \quad (8)$$

$$\sum_{\text{layer } k} p_k(i, j) = N_k P_k \quad (9)$$

where N_{k-1} and N_k are the number of pixels at layers $k-1$ and k respectively.

Replacing Eq. 9 in Eq. 7, the correction formula for $P(n, m)$ is then calculated as follows:

$$NP(n, m) = \sum_{\text{layer } k-1} p_{k-1}(i, j) + N_k P_k \quad (10)$$

$$\hat{P}_k(n, m) = \frac{NP(n, m) - \sum_{\text{layer } k-1} p_{k-1}(i, j)}{N_k} \quad (11)$$

where $\hat{P}_k(n, m)$ is the corrected value of the backprojection. Recursive application of Eq. 11 into Eq. 6 leads to the reconstruction. For each iteration, the upper part of Eq. 11 should be positive to guarantee the convergence to a solution.

3 Results

3.1 Forward Problem

Figure 3 shows the ultrasonic sinogram formed by 90 observation angles (angular step of 4°). Ray theory was applied without taking into account the attenuation in the different media. The color of each pixel corresponds to the slowness measured between two elementary sensors. Each line of the matrix corresponds to a projection.

3.2 Reconstruction and processing – Inverse Problem

Figure 4 shows the reconstructed object associated to each inversion algorithm. The reconstructed objects are smaller with respect to the original phantom. The theoretical number

of pixels that allow to reconstruct the scanned area with 90 emitter positions is 4005 [8]. The optimal size of the associated image is then 72×72 pixels. Note that the quality of the reconstructions obtained in Figure 4 is partly due to the fact that the forward problem and inverse problem involve the same approximate theory of straight ray propagation.

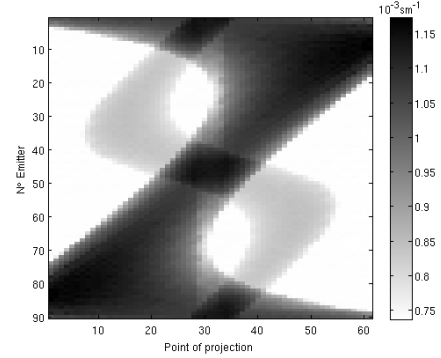


Figure 3: Simulated ultrasonic sinogram.

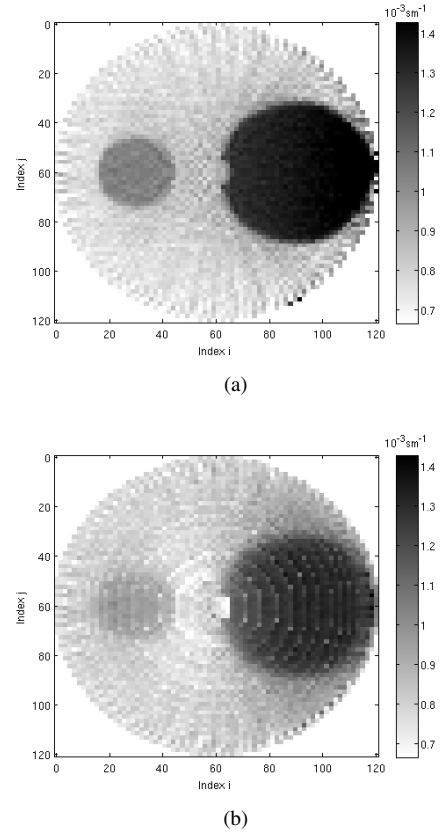


Figure 4: Reconstruction by: a) Filtered backprojection; b) Layer Stripping

Figure 5 shows the uncertainty of the linear model $Y=aX+b$ that compares the reconstructed measured slowness (X = projections of the reconstructed image (depend of the algorithm)) with respect to initial measured values (Y = projections of the phantom). The analysis were carried out with a confidence interval of 95% and each test was realized for the reconstruction for a given number of sensors. Figure 6 shows the mean of absolute deviations (mean deviation per pixel) between the reconstructed image and the phantom. The analysis was carried out by linear interpolation of the reconstructed image to the size of the phantom and comparing the deviation pixel

¹Size of the phantom and reconstructed image are different.

per pixel. When noise is not taken into account, both figures show that when this range of sensors (24 - 96) is used, the uncertainties decrease. Because the observations for further than 96 sensors were not tested, conclusion about the asymptotic behavior was not established. Reconstructions by the Layer Stripping algorithm are less performing than those carried out by the inversion by FBP. For a scan with 90 sensors, the respective uncertainties of the linear model were 7.2% (FBP) and 12.6% (LS). The mean deviations per pixel were about $0.079 \times 10^{-3} \text{sm}^{-1}$ (FBP) and $0.124 \times 10^{-3} \text{sm}^{-1}$ (LS); to be compared with the mean pixel value of $0.92 \times 10^{-3} \text{sm}^{-1}$ inside the scanned area of the phantom. For each one of these figures the slopes of each pair of curves are similar. Both inversion methods present similar behavior according to the number of sensors used for a given scan.

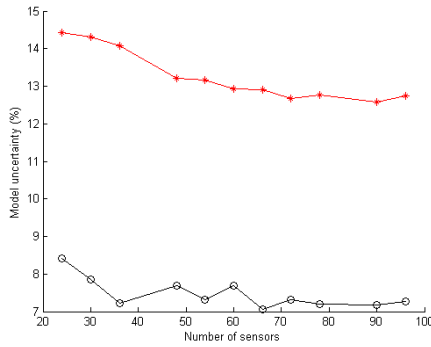


Figure 5: Linear model uncertainty according to the number of sensors for: o Filtered backprojection, * Layer Stripping

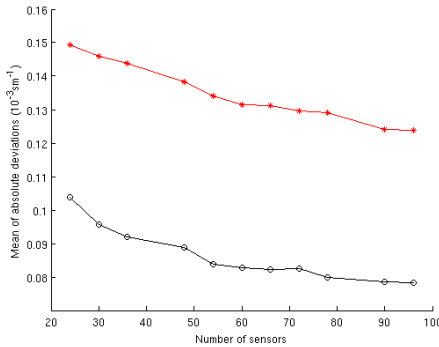


Figure 6: Mean deviation per pixel according to the number of sensors for: o Filtered backprojection, * Layer Stripping

Figures 7 and 8 show respectively the evolution of the linear model uncertainty and of the mean deviation per pixel when Gaussian noise is present for the same scan with 90 sensors. As noise increases, the uncertainties do it as well, but the behavior for the two inversion methods is different. The slopes of the curves of the uncertainties for the reconstructions by FBP are more sensitive to noise than for those by Layer Stripping. From about 20% of noise, the mean deviation per pixel for Layer Stripping is lower than for the FBP. For example at 30% of noise, linear model uncertainties are 15.7% (FBP) and 16.8% (LS), and are related to $0.209 \times 10^{-3} \text{sm}^{-1}$ and $0.173 \times 10^{-3} \text{sm}^{-1}$ deviation per pixel respectively.

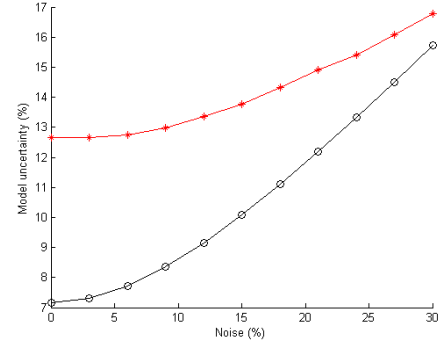


Figure 7: Linear model uncertainty according to the percentage of noise considered for: o Filtered backprojection, * Layer Stripping

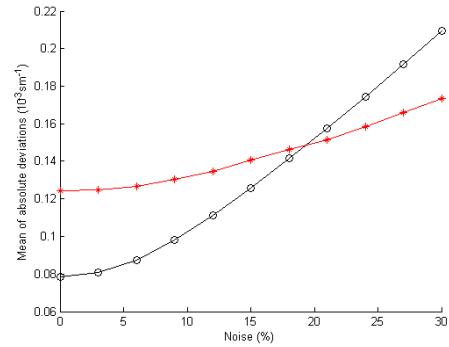


Figure 8: Mean deviation per pixel according to the percentage of noise considered for: o Filtered backprojection, * Layer Stripping

4 Conclusion

A new inversion algorithm has been presented as well as first numerical results. The tests consisted to simulate travel time tomography with the aim to compare the inversion of numerical data by Layer Stripping in relation to the inversion by Filtered Backprojection (reference method). These simulations depended of the experimental set-up of the ultrasonic tomograph and assumptions for the numerical phantom. For this first approach the phantom was assumed to be a cylindrical homogeneous isotropic medium with defects. Ray theory was applied without taking into account the attenuation. Quantitative analysis included the comparison of the uncertainties of the projections and slowness values of the reconstructed images with respect to the phantom. The first analysis showed that if noise is not taken into account, as more sensors are used for a scan, uncertainties decrease. Both inversion algorithms presented similar behavior according to the number of sensors. A general conclusion about this behavior was not established because tests were developed for a specific range of number of sensors. The results showed that if noise is not taken into account, uncertainties for Layer Stripping are greater than for FBP. The second analysis showed that, for a given scan, as noise increases, uncertainties do it as well, however the reconstructions by the FBP became more sensitive than those by Layer Stripping.

These results are the first step for further research in numerical modeling and experimental testing with samples of trees. In this paper it was underlined that the approach by Layer Stripping could be adapted to trees because it can be

associated to their 2D annular structure. A next step in numerical modeling should be the choice of a phantom with a concentric layer geometry. In relation to the inversion algorithms, because the actual challenge in tree imaging is the choice of the effective method to inverse scattered data, several reconstruction methods, from analytical to algebraic, should be also tested. Experimental tests using our tomographic device are also planned to be carried out.

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